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Title: Expanding the possibilities of electrografting modification of voltammetric sensors through two complementary strategies

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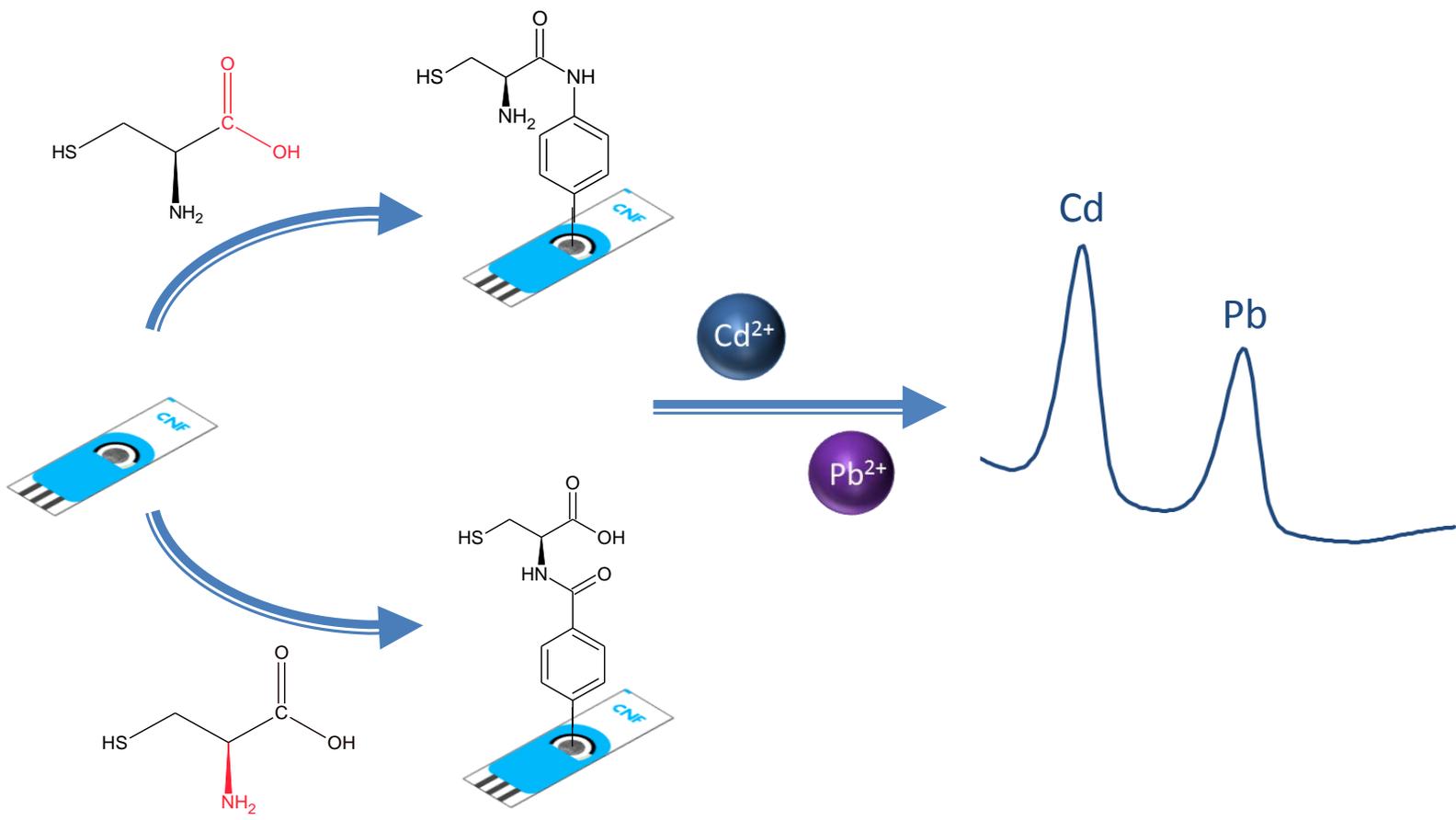
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Abstract: Two different modification strategies by means of aryl diazonium salt electrografting were compared for the development of voltammetric sensors. In this sense, L-cysteine was immobilized onto a screen-printed carbon-based electrode surface through either its -NH<sub>2</sub> or its -COOH group and the performance of the resulting modified sensors was tested for the simultaneous determination of Pb(II) and Cd(II) by anodic stripping voltammetry. The results obtained indicate that attachment through the -COOH group of cysteine, despite being a much less frequent electrografting strategy, improves the analytical performance of the resulting sensor achieving lower LODs, at low  $\mu\text{g L}^{-1}$  levels, for Cd(II) and Pb(II). Furthermore, this strategy allows the quantification of both metal ions below the legal limits established by the European Water Framework Directive, which represents a great improvement with respect to similar sensors reported in the literature.



1 Expanding the possibilities of electrografting modification of  
2 voltammetric sensors through two complementary strategies  
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28 **ABSTRACT**  
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31 Two different modification strategies by means of aryl diazonium salt electrografting  
32 were compared for the development of voltammetric sensors. In this sense, L-cysteine  
33 was immobilized onto a screen-printed carbon-based electrode surface through either its  
34  $-NH_2$  or its  $-COOH$  group and the performance of the resulting modified sensors was  
35 tested for the simultaneous determination of Pb(II) and Cd(II) by anodic stripping  
36 voltammetry. The results obtained indicate that attachment through the  $-COOH$  group  
37 of cysteine, despite being a much less frequent electrografting strategy, improves the  
38 analytical performance of the resulting sensor achieving lower LODs, at low  $\mu g L^{-1}$   
39 levels, for Cd(II) and Pb(II). Furthermore, this strategy allows the quantification of both  
40 metal ions below the legal limits established by the European Water Framework  
41 Directive, which represents a great improvement with respect to similar sensors reported  
42 in the literature.  
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**Keywords:** electrochemical grafting, peptide-modified sensors, screen-printed electrodes, stripping voltammetry, metal determination

## 1. INTRODUCTION

The problems associated with metal ions contamination have been known for years. During the last decades, metal emissions have significantly decreased, mainly due to their banning in some specific products (e.g. lead in gasoline or mercury regulations) or the decrease of their use and/or smelting [1,2]. However, the amount of metals emitted to the environment is still preoccupying and this, coupled to their non-biodegradable character, makes it still important to develop new analytical methods for the determinations of *on-site* trace metal ions.

Among all the available analytical techniques for metal ions determination, electrochemical techniques and, more specifically anodic stripping voltammetry (ASV), are particularly suitable. ASV measurements fulfil all the analytical requirements (high reproducibility and repeatability, low detection limits, high sensitivity, multielement determination...) and at the same time provide fast measurements with relatively low cost and portable equipment [3]. These last features are further enhanced by the coupling of ASV measurements with screen-printed electrodes (SPE), which are miniaturized, versatile, disposable and economical devices that can be mass-produced in a reproducible manner [4,5].

ASV measurements are strongly influenced by the chosen working electrode. Several types of working electrodes have been successfully reported for metal ion determination including metal films, sputtered electrodes, chemically modified electrodes, biosensors and metal nanoparticles or carbon nanostructured electrodes [6–12].

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Among all of these, chemically modified electrodes present the advantage that sensitivity and selectivity can be regulated by the incorporation of a convenient functional group onto the electrode surface. In this sense, several types of complexing agents such as EDTA [13–15], dimethylglyoxime [16], crown ethers [17,18] or thiolic compounds [19–22] have been used as electrode modifiers for metal ion determination. In particular, peptides are effective ligands for a great variety of metal ions because they contain a large number of potentially donor atoms. In any peptide, a metal ion can interact through the amino groups, the amide nitrogen and/or the carboxylic group present on its backbone and, additionally, this peptide-metal interaction can be further enhanced by other donor groups present in the side chains. This would be the case, for example, of thiol-rich peptides [23,24].

A good strategy reported in the literature for the immobilization of peptides and ligands in general onto carbon surfaces is based on the aryl diazonium salt electrografting [25]. This strategy allows the covalent linking of the modifier to the surface providing structural flexibility, chemical stability and control on the immobilization orientation and resulting in sensors with great reproducibility and durability [26]. Although carbon surfaces can be functionalized with different aryl diazonium salts, the most usual electrografting approach found in the literature is based on the *in-situ* generation of 4-carboxybenzenediazonium, which results on the functionalization of the electrode surface with carboxylic groups that allows the immobilization of modifiers containing an amino group through a peptide bond facilitated by cross-linking agents. A less common electrografting approach is based on the *in-situ* generation of 4-nitrobenzenediazonium. In this case, the electrode surface is functionalized with amino groups allowing the immobilization of modifiers through different functional groups such as carboxylic acids.

1 In order to compare these two electrografting based- strategies for sensor modification,  
2 in this work L-cysteine (L-Cys) was immobilized onto a screen-printed carbon-based  
3 electrode surface through either the generation of 4-carboxybenzenediazonium or 4-  
4 nitrobenzenediazonium and the performance of the resulting electrodes was studied for  
5 the simultaneous determination of Cd(II) and Pb(II).  
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## 11 12 13 14 15 16 **2. EXPERIMENTAL**

### 17 18 19 **2.1 Chemicals**

20 Hydrochloric acid, acetic acid, sodium acetate, 2-(N-morpholino)-ethanesulfonic acid  
21 (MES) and potassium ferrocyanide were supplied by Merck (Darmstadt, Germany).  
22 N-(3-dimethylaminopropyl)-N'-ethylcarbodiimide hydrochloride (EDC), N-  
23 hydroxysulfosuccinimide (sulfo-NHS), 4-nitroaniline (PNA), 4-aminobenzoic acid  
24 (ABA), sodium nitrite, potassium dihydrogen phosphate, sodium monophosphate and  
25 L-cysteine (L-Cys) with a purity greater than 99% were obtained from Sigma-Aldrich  
26 (St. Louis, MO, USA). Potassium ferricyanide was purchased from Panreac (Barcelona,  
27 Spain). Cd(II) and Pb(II) stock solutions  $10^{-2}$  mol L<sup>-1</sup> were prepared from  
28 Cd(NO<sub>3</sub>)<sub>2</sub>·4H<sub>2</sub>O and Pb(NO<sub>3</sub>)<sub>2</sub>·4H<sub>2</sub>O respectively and standardized complexometrically  
29 [27]. In all cases analytical grade reagents were used and solutions were prepared with  
30 ultrapure water (Milli-Q plus 185 system, Millipore).  
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### 51 **2.2 Apparatus**

52 Stripping voltammetric measurements were carried out on an Autolab System  
53 PGSTAT12 (EcoChemie, The Netherlands) attached to a Metrohm 663 VA Stand  
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1 (Metrohm, Switzerland). GPES software version 4.9 (EcoChemie) was used for data  
2 acquisition.  
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5 Ag|AgCl|KCl (3 mol L<sup>-1</sup>) reference electrode and Pt wire counter electrode were  
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7 acquired from Metrohm (Switzerland). A carbon nanofiber screen-printed electrode  
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9 (SPCNFE, 4 mm diameter), supplied by Dropsens (Spain), was modified with Cys and  
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11 used as working electrode. A flexible cable (ref. CAC, DropSens) was employed for the  
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13 connection of screen-printed electrodes.  
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17 pH measurements were carried out on a Crison micro pH 2000 pH-meter and all  
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19 measurements were performed in a glass cell at room temperature (20 °C) without  
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21 oxygen removal.  
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## 24 25 **2.3 Preparation of modified SPEs**

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28 Cys modified SPEs were prepared by two different methods according to the schemes  
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30 shown in Figure 1. Both methods are based on the electrografting of an aryl diazonium  
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32 salt followed by the covalent immobilization of Cys.  
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### 36 *2.3.1 Preparation of (ABA)Cys-SPCNFE*

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38 The preparation of (ABA)Cys-SPCNFE is described elsewhere [28]. Briefly, 2  
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40 mmol L<sup>-1</sup> NaNO<sub>2</sub> was added drop by drop to a cooled solution of 73 mmol L<sup>-1</sup> of ABA  
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42 in 1 mol L<sup>-1</sup> aqueous HCl and left to stir in an ice bath for 30 min to generate the aryl  
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44 diazonium salt. Then, the electrografting process was conducted in this solution by CV;  
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46 applying 15 cycles from 0 to -1 V at 200 mV s<sup>-1</sup>.  
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51 After rinsing the electrodes with Mili-Q water and ethanol, the carboxyl groups  
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53 generated on the electrode surface were activated by dropping 10 µL of a 5 mg mL<sup>-1</sup>  
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55 EDC and 7.5 mg mL<sup>-1</sup> sulfo-NHS solution in 0.1 mol L<sup>-1</sup> MES buffer (pH 4.5) onto the  
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57 functionalized electrodes and leaving it to incubate for 1 h. Finally, 10 µL of a 2.9  
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1 mg/100  $\mu\text{L}$  Cys solution in 0.1 mol  $\text{L}^{-1}$  MES buffer (pH 4.5) were dropped onto the  
2 electrode and left to react overnight at 4  $^{\circ}\text{C}$ .  
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### 4 5 2.3.2 Preparation of (PNA)Cys-SPCNFE 6

7 10 mmol  $\text{L}^{-1}$   $\text{NaNO}_2$  was added drop by drop to a cooled solution of 12 mmol  $\text{L}^{-1}$  of  
8 PNA in 1 mol  $\text{L}^{-1}$  aqueous HCl and left to stir in an ice bath for 30 min to generate the  
9 aryl diazonium salt. Then, the electrografting process was conducted in this solution by  
10 CV; applying 15 cycles from 0 to -1 V at 200  $\text{mV s}^{-1}$ .  
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13 After rinsing the electrodes with Mili-Q water and ethanol, the nitro groups were  
14 reduced with 5 cycles of CV from -0.4 to -1.2 V at 200  $\text{mV s}^{-1}$  in 10 mmol  $\text{L}^{-1}$  HCl.  
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17 After CV, the electrodes were rinsed again with Mili-Q water and ethanol.  
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20 Finally, the amino groups reacted overnight at 4  $^{\circ}\text{C}$  with 10  $\mu\text{L}$  of a 2.9 mg/100  $\mu\text{L}$  Cys  
21 solution in 0.1 mol  $\text{L}^{-1}$  MES buffer (pH 4.5) previously activated with 8.25 mg/100  $\mu\text{L}$   
22 EDC and 5.25 mg/100  $\mu\text{L}$  sulfo-NHS for 1 h.  
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## 32 33 34 35 **2.4 Voltammetric measurements** 36

37 Differential pulse anodic stripping voltammetric (DPASV) measurements of Cd(II) and  
38 Pb(II) using (ABA)Cys-SPCNFE and (PNA)Cys-SPCNFE were performed in acetate  
39 buffer 0.1 mol  $\text{L}^{-1}$  pH 4.5 or 5, depending on the considered sensor, applying a  
40 deposition potential ( $E_d$ ) of -1.0 V for a deposition time of 120 s with stirring.  
41 Deposition was followed by a rest period ( $t_r$ ) of 5 s and a scan from -1.0 to -0.3 V with  
42 pulse times of 50 ms, pulse amplitudes of 100 mV and step potentials of 5 mV was  
43 recorded. In order to remove any remaining bound metals, an electrochemical cleaning  
44 stage consisting on the application of a conditioning potential ( $E_{\text{cond}}$ ) of 0 V for 60 s was  
45 introduced between measurements.  
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1 Electrode characterizations at different modification steps and pHs was performed by  
2 CV using 2 mmol L<sup>-1</sup> ferrocyanide/ferricyanide in 100 mmol L<sup>-1</sup> phosphate buffer as a  
3 redox probe. The potential was scanned from -0.5 to 0.7 V at 100 mV s<sup>-1</sup>.  
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### 9 **3. RESULTS AND DISCUSSION**

#### 10 **3.1 Electrodes modification**

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13 As a first step, aryl diazonium salts were generated *in situ* from ABA and PNA in 1 mol  
14 L<sup>-1</sup> HCl and grafted onto the SPCNFE surface. CV measurements observed during the  
15 reduction of the diazonium salts are presented in figure 2a and 2b for 4-  
16 carboxybenzenediazonium and 4-nitrobenzenediazonium respectively. In both cases, a  
17 broad irreversible peak that decreases with every scan can be observed. This decrease in  
18 the peak intensity is due to the formation of an organic layer on the surface of the  
19 electrode, which prevents the access of the diazonium cations [25].  
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33 Additionally, for the preparation of (PNA)Cys-SPCNFE, the electrografting process  
34 was followed by the reduction of the nitro groups generated onto the electrode surface.  
35 This reduction was performed by CV in 0.01 mol L<sup>-1</sup> HCl and, as it is shown in figure  
36 2c, a broad irreversible cathodic peak can be observed at -0.775 V, which is  
37 characteristic of the six electron reduction reaction of the nitro groups to the amino  
38 groups [29]. The disappearance of this peak in the following cycles shows that the  
39 reduction of the nitro groups was completed.  
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51 These steps allowed the generation of either carboxylic or amino groups onto the  
52 electrode surface, which were later used to immobilize Cys through the formation of a  
53 peptide bond assisted by EDC/sulfo-NHS crosslinking agents. This way, (ABA)Cys-  
54 SPCNFE has a free thiol and a free carboxylic group whereas in (PNA)Cys-SPCNFE  
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1 the thiol and amino groups are available, which will be protonated or deprotonated  
2 depending on the working pH value (Figure 1).  
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### 5 **3.2 Effect of pH on the electrode surface**

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8 The immobilization of Cys through the amino group in (ABA)Cys-SPCNFE and  
9 through the carboxylic group in (PNA)Cys-SPCNFE, both assisted by EDC/sulfo-NHS  
10 crosslinking agents, leads to the availability of different pH-dependent groups for each  
11 electrode. Thus, the electrode response was studied at different pHs.  
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18 For this purpose, CV measurements were carried out in a 2 mmol L<sup>-1</sup>  
19 ferrocyanide/ferricyanide at several pHs. Since ferrocyanide/ferricyanide is a non-pH  
20 dependent redox probe, the difference in the peak intensities can be explained by the  
21 electrostatic interactions of the electrode surface and the redox probe. Figure 3 shows  
22 the evolution of anodic current peaks vs. pH for (ABA)Cys-SPCNFE, (PNA)Cys-  
23 SPCNFE and bare SPCNFE. As it can be seen, at pH 3 the highest response corresponds  
24 to (PNA)Cys-SPCNFE, which could be associated to the positive charge of the amino  
25 group in **D** that creates a favourable electrostatic interactions with [Fe(CN)<sub>6</sub>]<sup>3-/4-</sup>. In both  
26 (ABA)Cys-SPCNFE and bare SPCNFE the surface charge should be neutral and the  
27 lower response for (ABA)Cys-SPCNFE could be attributed to the presence of the  
28 cysteine-based layer that hinders the access of [Fe(CN)<sub>6</sub>]<sup>3-/4-</sup>. As the pH increases from  
29 3 to 6, a current decrease is observed for both (ABA)Cys-SPCNFE and (PNA)Cys-  
30 SPCNFE. Although this behaviour cannot be associated to the theoretical acid-base  
31 equilibriums, a possible explanation could be related to the first steps of the  
32 modification procedure. As it can be seen in Figure 1, in the case of (ABA)Cys-  
33 SPCNFE and (PNA)Cys-SPCNFE, the electrode surface is functionalized with benzoic  
34 acid and aniline units, respectively, prior to cysteine attachment. Although most of  
35 these units are later linked to cysteine through the EDC/sulfo-NHS crosslinking agents,  
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it is possible that some of them remain unmodified. These unmodified units would have theoretical  $pK_a$  values of 4.2 (benzoic acid) and 4.9 (aniline), which would explain the above-mentioned current decrease. In the case of bare SPCNFE, no surface functionalization was performed and, therefore, this current decrease is not observed.

In the pH region from 6 to 11 the slight current decrease observed can be explained by the acid-base equilibriums of cysteine forms. Particularly, in the case of (ABA)Cys-SPCNFE, this decrease can be associated to the deprotonation of the thiol group (**B – C**), with an experimental  $pK_a$  value, calculated from the  $dI/dpH$  vs. pH, close to 9. On the other hand, for (PNA)Cys-SPCNFE only one experimental  $pK_a$  value close to 8 was observed, which could be attributed to the loss of both amino (**D – E**) and thiol (**E – F**) protons.

### 3.3 Application to the determination of metal ions

Both (ABA)Cys-SPCNFE and (PNA)Cys-SPCNFE were tested for the determination of Pb(II) and Cd(II) as a model metal ion system by DPASV. First of all, some experimental parameters including pH,  $E_d$  and  $t_d$  were optimized. Figure 4 shows the response evolution vs pH of both considered sensors for a solution containing  $50 \mu\text{g L}^{-1}$  of Pb(II) and Cd(II). pH is a critical parameter in this type of determination since it affects most of the processes involved such as protonation/deprotonation of functional groups with affinity for metal ions (-SH, -NH<sub>2</sub>, -COOH), electrostatic interactions between the metal ion and the electrode surface and metal hydrolysis. For (ABA)Cys-SPCNFE the optimal pH was established at 5, which can be justified by presence of COO<sup>-</sup> groups on the electrode surface that allow a favourable electrostatic interaction with the metal ions. At lower pHs this COO<sup>-</sup> groups are protonated and this electrostatic interaction is not present whereas at higher pHs metal ion hydrolysis can be observed. A similar behaviour is shown by (PNA)Cys-SPCNFE, although in this case the lower

1 response at pHs lower than 4 could be explained by the non-favourable electrostatic  
2 interaction with metal ions caused by the positively charged protonated aniline units  
3 present on the surface.  
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7 Regarding  $E_d$ , different voltammetric measurements were carried out from -1.4 V to  
8 -1.0 V in a solution containing  $50 \mu\text{g L}^{-1}$  of Pb(II) and Cd(II) using both (ABA)Cys-  
9 SPCNFE and (PNA)Cys-SPCNFE. In both cases, the highest current response for both  
10 Cd(II) and Pb(II) was found at an  $E_d$  of -1.0 V and, therefore, this value was selected  
11 for further experiments. Finally,  $t_d$  was also studied from 30 to 300 s and a  $t_d$  of 120 s  
12 was selected as a compromise between peak area and analysis time.  
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23 Once the experimental conditions were optimized the analytical performance of both  
24 sensors was studied considering repeatability, reproducibility, sensibility, linear range  
25 and limits of detection (LOD) and quantification (LOQ). All these values are  
26 summarized in Table 1.  
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33 Repeatability was computed from 5 repetitive measurements carried out with the same  
34 sensor on a solution containing  $50 \mu\text{g L}^{-1}$  of Pb(II) and Cd(II) in acetate buffer achieving  
35 similar RSD(%) values for both metal ions and both sensors, lower than 1.6 % in all  
36 cases. Reproducibility was estimated from the slope of three independent calibration  
37 curves carried out from 1 to  $150 \mu\text{g L}^{-1}$  of Pb(II) and Cd(II) using three different  
38 sensors. The obtained values were lower than 1.3 % in all cases, which proves that both  
39 modification strategies produce very reproducible sensors, being slightly better in the  
40 case of (PNA)Cys-SPCNFE.  
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53 Simultaneous Pb(II) and Cd(II) calibration curves were performed at the optimal  
54 experimental conditions from 1 to  $150 \mu\text{g L}^{-1}$  using both (ABA)Cys-SPCNFE and  
55 (PNA)Cys-SPCNFE. As it can be seen in Figure 5 two separate and well-defined peaks  
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1 were obtained for both considered metal ions. Similar shapes and intensities were  
2 obtained for Cd(II) using both sensors whereas in the case of Pb(II) a more gaussian-  
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4 shaped peak with higher intensities was observed using (PNA)Cys-SPCNFE.  
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7 Regarding sensitivity, computed as the slope of the calibration curve, both sensors  
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9 present a higher sensitivity for Cd(II) than for Pb(II) which is in agreement with the  
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11 hard-soft classification scheme, where softer ligands such as thiols present more affinity  
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13 to softer metals like Cd(II) [23]. This higher preference for Cd(II) is accentuated in the  
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15 case of (ABA)Cys-SPCNFE. On the other hand, LODs and LOQs, calculated as three  
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17 and ten times the standard deviation of the intercept over the slope of the calibration  
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19 curve respectively, were in all cases at  $\mu\text{g L}^{-1}$  levels. It should be pointed out that both  
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21 sensors are able to quantify Pb(II) at lower concentrations than the established legal  
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23 limit ( $10 \mu\text{g L}^{-1}$  according to the European Water Framework Directive 2000/60/EC)  
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25 whereas only (PNA)Cys-SPCNFE can quantify Cd(II) at the more demanding limit  
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27 established by the same directive for this metal ( $5 \mu\text{g L}^{-1}$ ). This fact could be justified by  
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29 the presence of amino groups in (PNA)Cys-SPCNFE that also have a strong binding  
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31 preference for soft metals like Cd(II) [23].  
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40 Therefore, considering both peak shapes and analytical performance, we can conclude  
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42 that attaching cysteine through its carboxylic group, i.e. (PNA)Cys-SPCNFE, is a better  
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44 option than attaching it through the amino group since it provides a better sensor for the  
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46 determination of metal ions at trace concentration levels, being able to simultaneously  
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48 quantify both Cd(II) and Pb(II) at the legal limits established by the European Water  
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50 Framework Directive. Moreover, it should be highlighted that the developed (PNA)Cys-  
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52 SPCNFE sensor clearly improves the results previously reported for peptide-modified  
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54 sensors [19–21,30], none of which provides a LOQ below the legal limit, without  
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increasing the analysis time ( $t_d$  is the same or even lower than that used in the cited works).

In general terms, after studying the behaviour of both electrografting approaches, it can be said that the approach based on 4-nitrobenzenediazonium, although being less common, is not only an alternative strategy to the most usual electrografting procedure based on 4-carboxybenzenediazonium but can also give rise to improved sensors in some cases. It should also be pointed out that, although requiring an additional modification step to reduce the nitro groups to amino groups (Figure 1), the total sensor development time is similar or even slightly shorter than the procedure based on 4-carboxybenzenediazonium, with the additional advantage of allowing the attachment of modifiers with carboxylic groups that otherwise would require the use of a lysine spacer to assist their immobilization with the more usual electrografting based on 4-carboxybenzenediazonium.

#### 4. Conclusions

At the view of the obtained results we can conclude that Cys was successfully linked to the SPCNFE surface through both its  $-NH_2$  and  $-COOH$  groups using aryl diazonium electrografting based strategies giving rise to two different sensors. The sensor performance was studied as a function of pH showing slightly different behaviour according to the free functional groups available in each case. Moreover, both sensors were analytically tested for metal ion determination using Pb(II) and Cd(II) as a model system. Firstly, the working pH was established, being 4.5 and 5.0 the optimal value for (PNA)Cys-SPCNFE and (ABA)Cys-SPCNFE respectively. At these pH conditions, metals are not affected by hydrolysis and the electrostatic interactions between metal ions and the electrode surface are favourable.

1 From an analytical point of view, although both developed sensors are very repetitive  
2 and reproducible and can be used for a large number of measurements without signs of  
3 degradation, (PNA)Cys-SPCNFE presents a better voltammetric behaviour conferred by  
4 the better shaped Pb(II) peak. Both (PNA)Cys-SPCNFE and (ABA)Cys-SPCNFE are  
5 sensible sensors that are able to detect Pb(II) and Cd(II) at trace levels with LODs  
6 around 1 and 2  $\mu\text{g L}^{-1}$  for Pb(II) and Cd(II) respectively, resulting in suitable sensors for  
7 the detection of Pb(II) and Cd(II) at very low concentrations. However, (PNA)Cys-  
8 SPCNFE presents the additional feature of being capable of quantifying both metal ions  
9 below the legal limits established by the European Water Framework Directive, which  
10 represents a great improvement with respect to similar sensors reported in the literature.  
11 Thus, despite being a much less common electrografting strategy for the development of  
12 voltammetric sensors, the approach based on 4-nitrobenzenediazonium is also a  
13 valuable procedure that should be further taken into account.

14 Finally, it should be pointed out that the combination of both electrografting approaches  
15 clearly expands the versatility of the covalent modification strategies for the  
16 development of voltammetric sensors since it allows the attachment of modifiers with  
17 different functional groups, therefore broadening the list of modifiers that can be  
18 covalently linked to an electrode surface.

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23 the Water Research Institute (IdRA) of the University of Barcelona for its support.

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**Table 1.** Calibration data for the simultaneous determination of Pb(II) and Cd(II) on (ABA)Cys-SPCNFE and (PNA)Cys-SPCNFE at acetate buffer pH 5 and 4.5 respectively applying an  $E_d$  of -1.0V and a  $t_d$  of 120 s. Standard deviations are denoted by parenthesis

	(ABA)Cys-SPCNFE		(PNA)Cys-SPCNFE	
	Cd(II)	Pb(II)	Cd(II)	Pb(II)
<b>Sensitivity (a.u. <math>\mu\text{g}^{-1} \text{L}</math>)</b>	5.39 (0.05)	2.75 (0.01)	4.63 (0.03)	3.44 (0.01)
<b><math>R^2</math></b>	0.998	0.999	0.999	1.000
<b>Linear range (<math>\mu\text{g L}^{-1}</math>)<sup>a</sup></b>	7.3 – 153.9	3.7 – 153.9	4.6 – 153.9	3.4 – 153.9
<b>LOD (<math>\mu\text{g L}^{-1}</math>)</b>	2.2	1.1	1.4	1.0
<b>Repeatability (%)</b>	1.52	1.58	1.39	1.33
<b>Reproducibility (%)</b>	1.29	1.15	0.82	0.92

<sup>a</sup>LOQ was considered as the lowest value of the linear range.

Figure 1

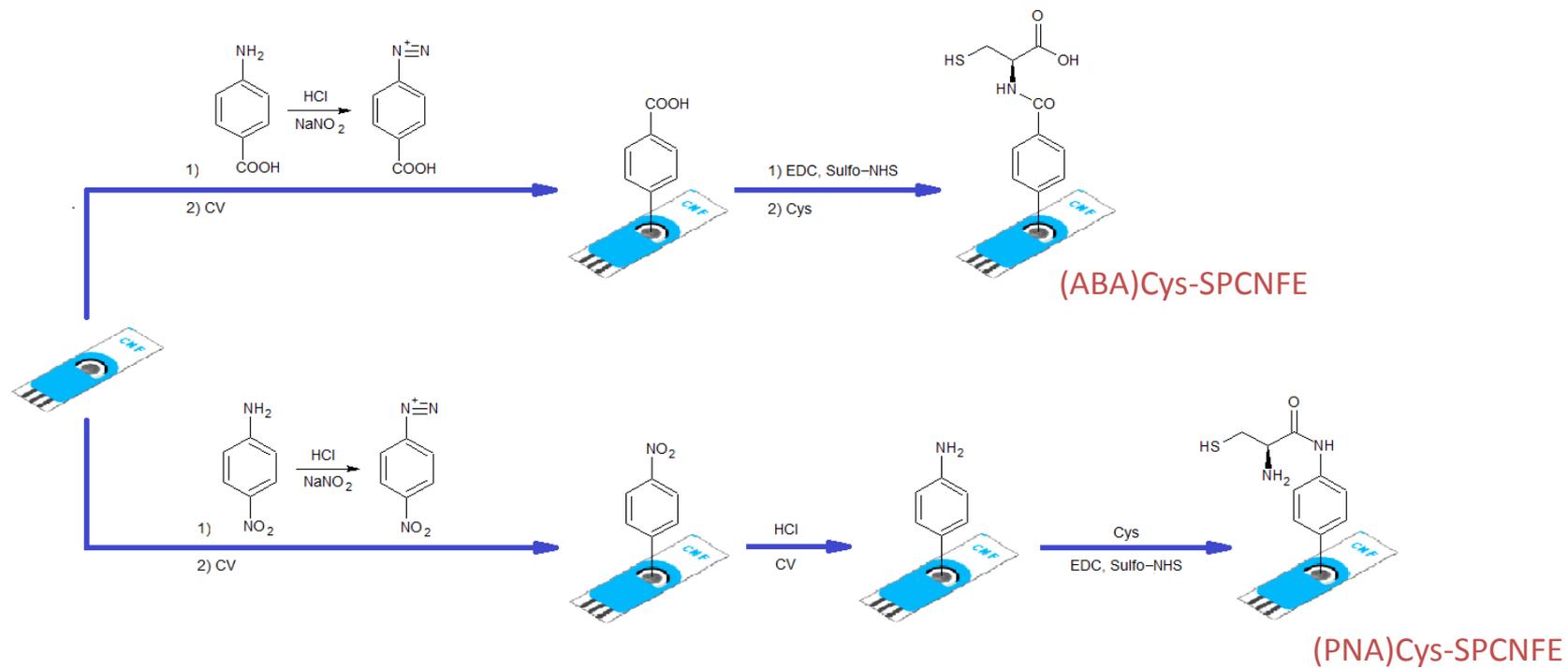


Figure 2

Figure 2

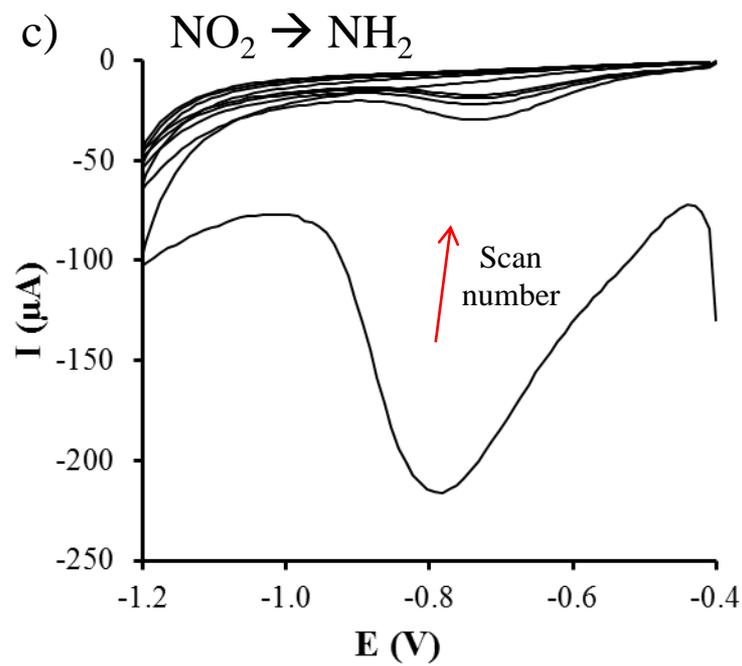
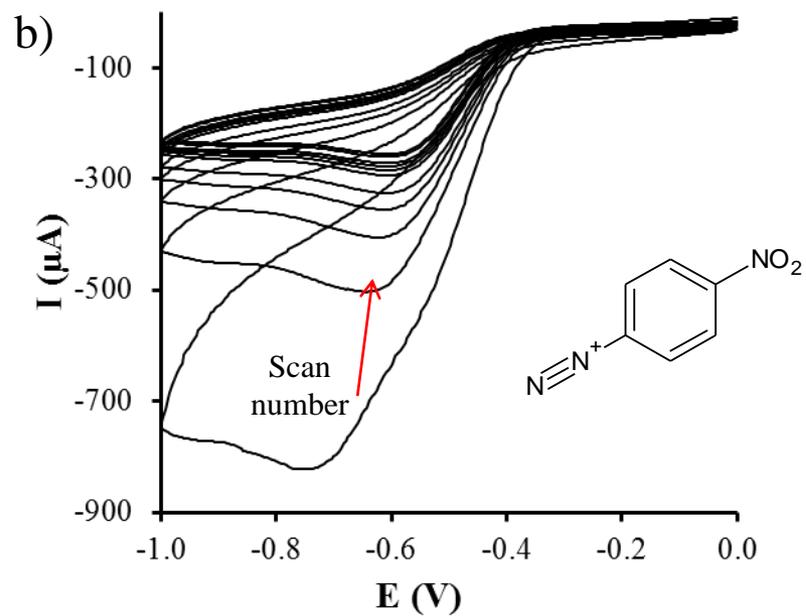
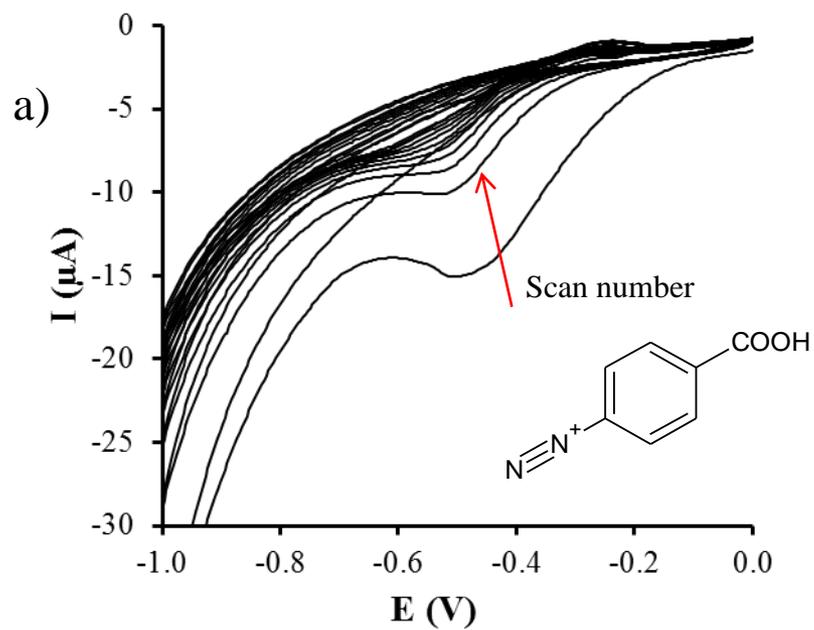
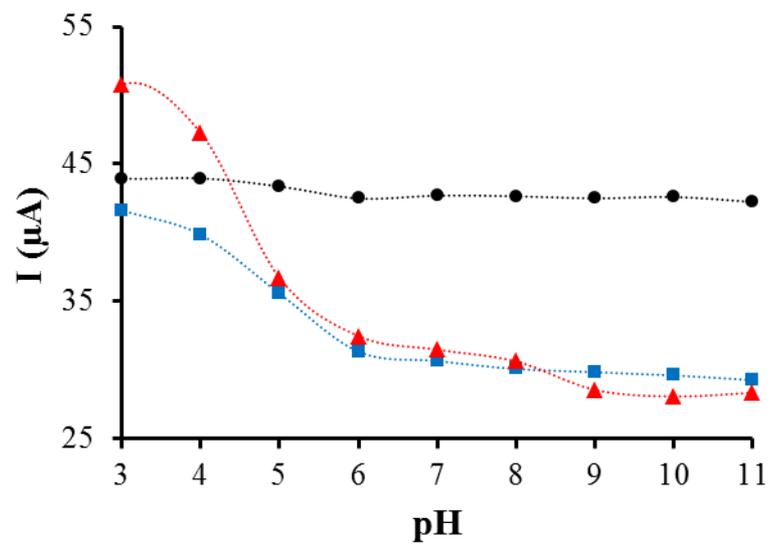
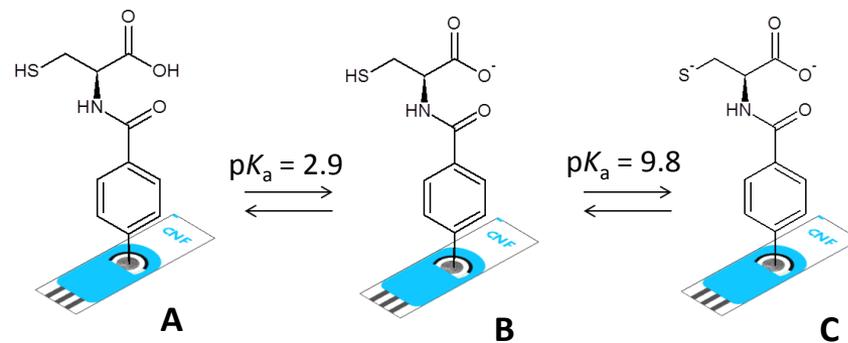


Figure 3



## (ABA)Cys-SPCNFE



## (PNA)Cys-SPCNFE

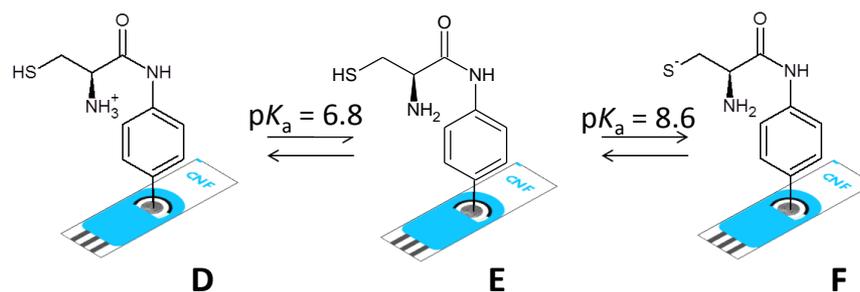


Figure 4

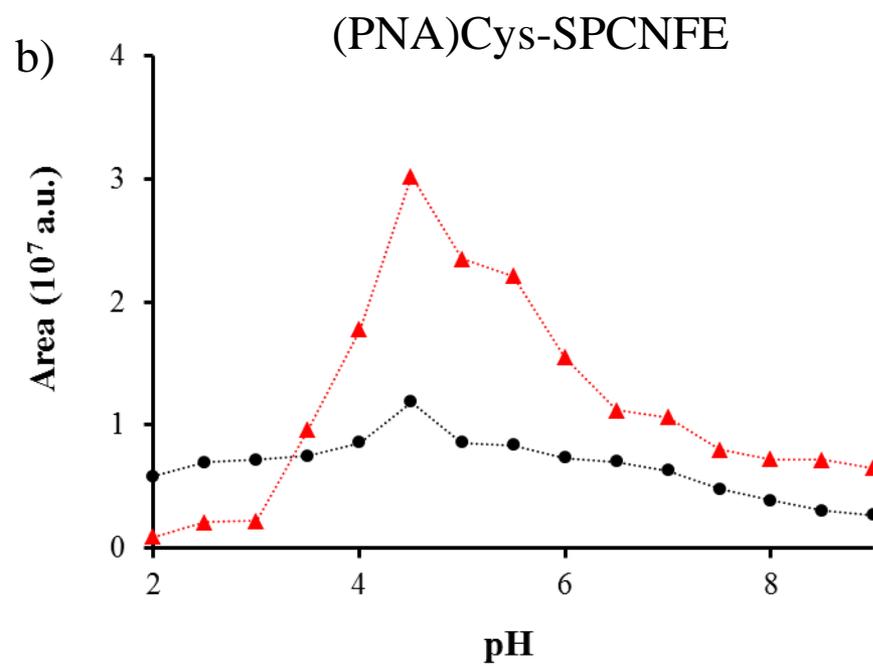
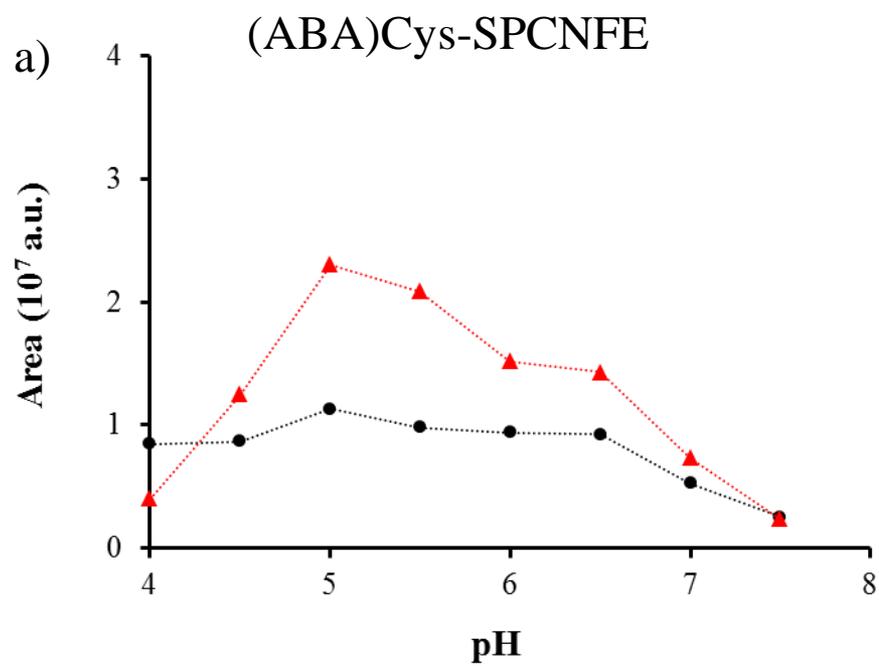


Figure 5

