

Latest advances in image processing for single particle analysis by electron cryomicroscopy and challenges ahead

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Abstract

Electron cryomicroscopy (cryo-EM) is essential for the study and functional understanding of non-crystalline macromolecules such as proteins. These molecules cannot be imaged using X-ray crystallography or other popular methods. Cryo-EM has been successfully used to visualize molecules such as ribosomes, viruses, and ion channels, for example. Obtaining structural models of these at various conformational states leads to insight on how these molecules function. Recent advances in imaging technology have given cryo-EM a scientific rebirth. Because of imaging improvements, image processing and analysis of the resultant images have increased the resolution such that molecular structures can be resolved at the atomic level. Cryo-EM is ripe with stimulating image processing challenges. In this article, we will touch on the most essential in order to build an accurate structural three-dimensional model from noisy projection images. Traditional approaches, such as k-means clustering for class averaging, will be provided as background. With this review, however, we will highlight fresh approaches from new and varied angles for each image processing sub-problem, including a 3D reconstruction method for asymmetric molecules using just two projection

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images and deep learning algorithms for automated particle picking.

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1. Introduction

Cryo-Electron microscopy (cryo-EM) of single particles has been established as a key technique for the elucidation of the three-dimensional structure of biological macromolecules. The *Nature Methods* Method of the Year (2015) and the Nobel Prize in Chemistry (2017) endorse this view. Cryo-EM is currently capable of achieving quasi-atomic resolution (1.8Å) in some specimens, and visualizing specimens with molecular weights below 100 kDa with a resolution better than 4Å [1]. Beside that, Cryo-EM can yield key insight into the dynamics of macromolecules [2, 3, 4], and it provides a solid base for structure-based drug design, although some technical problems in this arena remain open [5].

The main advances in the last five years have come from multiple sources: 1) more sensitive and faster detectors at the microscope, 2) faster and more robust image processing algorithms, and 3) more reproducible sample preparation techniques.

In this review we address the image processing algorithm developments of the last five years. To begin, we quickly summarize here the advances in the other aspects of EM (not covered in this review) that also affect the image quality:

- Image formation process. Much attention has been placed on better understanding of the physicochemical processes leading to radiation damage [6, 7, 8], beam induced movement [9, 10] characterizing camera noise (modeling the noise produced by sensors capturing EM images) [11, 12], modelling and correcting optical aberrations [13, 14, 15], especially the defocus gradient along the specimen [16, 17, 18], the charging effect [19, 20], the design and use of phase plates as a way to increase contrast [21, 22, 23], and single band imaging as a way to address the defocus gradient [24, 25, 26].

- 27 • Better detectors. Direct electron detectors have caused a quantum leap
28 in EM. The current trends include thinner back-ends as a way to reduce
29 the actual size of the point spread function, increased quantum efficiency
30 of the detector in order to increase its sensitivity, and faster readouts as
31 a way to better correct for the beam induced movement [27, 28].
- 32 • Better sample preparation. Research in sample preparation has focused
33 on increasing the sample stability [29] and reducing the amount of sam-
34 ple required for vitrification as a way to increase its freezing speed and
35 reproducibility [30, 31, 32, 33].

36 This paper is organized as follows: in Section 2 we review the advances
37 during the last five years in image processing algorithms for Single Particle
38 Analysis. In Section 3 we expose the current open problems in the field from
39 the algorithmic point of view, and present conclusions. A graphical summary
40 of the main topics discussed is shown in Figure 1. The blue arrows between 2D
41 Processing and 3D Analysis depict the cyclical nature of different stages - the
42 order of steps may vary from method to method.

43 **2. Recent Advances in Image Processing Algorithms for Single Par-** 44 **ticl Analysis**

45 In terms of software, large packages tend to be very inclusive, covering the
46 whole pipeline from image acquisition to the final 3D reconstruction (Relion [34],
47 Eman2 [35], Frealign and Cistem [36], Xmipp [37], Spider [38], Sparx [39], Bsoft
48 [40]). These packages even include small tools from other software providers
49 solving specific image processing problems. Two large integrative platforms
50 have appeared in the domain: Scipion [41] and Appion [42]. In these platforms,
51 the user may easily call different algorithms from different providers, and the
52 system automatically performs the necessary conversions. In recent years, many
53 engineering groups are contributing software that solve very specific problems
54 along the image processing pipeline. These tools tend to be incorporated in the
55 integrative platforms.

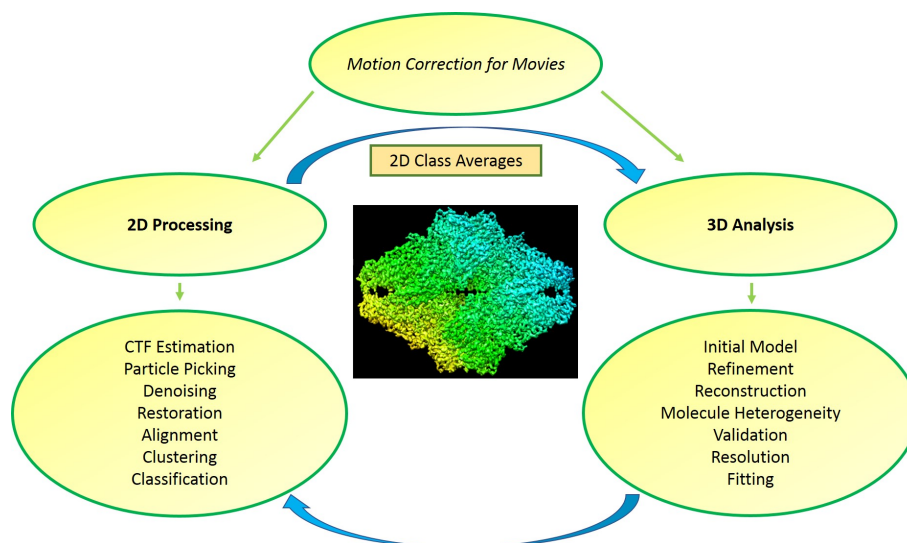


Figure 1: Summary of the main topics discussed in this review. Pictured is a 3D reconstruction of β -galactosidase (isosurface representation of Xmipp highres reconstruction.)

56 *2.1. Movies and Micrographs*

57 The contrast between the sample and its background is one of the factors
58 that determine the final quality of an image. Grant and Grigorieff [43] demon-
59 strated a method of using optimal exposure values to filter movie frames, yield-
60 ing images with improved contrast that lead to higher resolution reconstructions.
61 They were studying how quickly a large virus-like particle is damaged under the
62 electron beam. These experiments identified an optimum range of exposure to
63 electrons that provides the highest image contrast at any given level of detail.
64 Their findings were used to design an exposure filter that can be applied to the
65 movie frames. With higher contrast, greater levels of structural information can
66 be obtained. However, this increase in contrast requires the use of longer expo-
67 sure to the electron beam. To overcome this issue, instead of recording a single
68 image, it is possible to record movies in which the movement of the sample under
69 the electron beam can be tracked. The correction of specimen movement was
70 solved by a number of algorithms. Ripstein et al. [44] explained and compared
71 several of the most popular existing algorithms for computationally correcting

72 specimen movement including *Motioncorr* [45], *alignframes_lmbfgs* and *align-*
73 *parts_lmbfgs* [46], *Unblur* [43], and others, while summarizing all the advantages
74 of each technique.

75 While conceptually simple, the algorithms used to perform motion correction
76 vary widely, because each alignment routine uses different criteria to guide and
77 smooth the alignment. Through understanding the different options, we may
78 achieve insights to better design the next generation of alignment software.

79 McLeod et al. [47] presented a software package *Zorro*, which provides ro-
80 bust drift correction for dose fractionation by use of an intensity-normalized
81 cross-correlation and logistic noise model to weight each cross-correlation in the
82 multi-reference model and filter each cross-correlation optimally. Frames are re-
83 liably registered here with low dose and defocus. The package utilizes minimal
84 heuristics that minimizes the number of arbitrary input parameters required of
85 the user. The most critical input parameters, weighting of peak significance and
86 B-filter strength, are performed automatically.

87 Recently, a novel software tool *MotionCor2* [48] for anisotropic correction of
88 beam-induced motion was introduced. The algorithm is based on an experimen-
89 tally validated model that describes the sample motion as a local deformation
90 that varies smoothly throughout the exposure. It combines the correction of
91 both uniform whole-frame motion and anisotropic local motion, and it stream-
92 lines all the necessary preprocessing steps including bad pixel detection and
93 correction before the normal cryo-EM processing pipeline.

94 Another problem with movies is related to their acquisition using Direct
95 Electron Detector (DED), where non-negligible differences between the gain of
96 different sensor areas could be introduced. Therefore, approaches to estimate
97 the DED camera gain at the pixel level were developed. Afanasyev et al. [49]
98 assimilate the gain of the camera to the standard deviation of each pixel over
99 a large number of movies and prove this is a successful way of identifying dead
100 pixels. However, Sorzano et al. [50] showed that this approach does not provide
101 a consistent gain estimation; therefore, they introduced a different approach to
102 estimate the DED camera gain at each pixel from the movies. Their algorithm

103 iteratively refines the gain image using local smoothness of the histograms of
104 image rows and columns. A monitor of the gain estimate can be set to warn
105 the user if the residual acquisition gain goes beyond certain limits (defined by
106 the user as thresholds on its standard deviation and other percentile based
107 parameters.)

108 *2.2. 2D Processing*

109 *2.2.1. CTF Estimation*

110 An electron microscope, as with any other imaging device, has a number
111 of physical aberrations that distort the ideal projections, by modulating ampli-
112 tudes and phases of the recorded electrons. To reach the best resolution, it is
113 necessary to correct these distortions by estimating and correcting the contrast
114 transfer function (CTF). The fitting procedure consists in an iterative adjust-
115 ment minimizing the discrepancy between simulated and experimental power
116 spectral densities (PSD) using a non-linear optimization that depends on an
117 initial estimation of the model parameters, particularly the defocus.

118 Several improvements of the CTF estimation have been done during the last
119 years trying to improve the computation time and the accuracy, due to the
120 large amount of micrographs to analyze. A novel parameter-free approach has
121 been presented in [51] in which a fast way to recover the defocus and astigma-
122 tism of the CTF without the need of non-linear optimization procedures and
123 an initial defocus estimation is proposed. This method is available in Xmipp
124 3.0 [37]. Other software has been developed for the CTF estimation such as
125 CTFFIND4, which provides an improved version of CTFFIND3 that is faster
126 and more suitable for images collected using modern technologies such as dose
127 fractionation and phase plate [52]. Gctf accelerates the CTF estimation using
128 GPU. The main target of this is to maximize the cross-correlation of a sim-
129 ulated CTF with the logarithmic amplitude spectra of observed micrographs
130 after background subtraction. Also, an approach for local CTF refinement of
131 each particle in a micrograph or frames in a movie is provided to improve the
132 accuracy of CTF determination [53]. With the different programs available, it

133 is becoming more difficult to compare their results across several runs and to se-
134 lect the best parameters to measure the CTF quality. To address this difficulty,
135 a new parameter has been proposed in [54]. They introduce for this purpose
136 the so-called CTF resolution, where they measure the correlation falloff of the
137 calculated CTF oscillations against the normalized oscillating signal of data. It
138 is a robust metric to select the best parameters for each micrograph.

139 A novel phase contrast technique called the Volta Phase Plate (VPP) [21] has
140 been developed during the last years trying to get more contrast in the electron
141 micrographs. The phase shift brought in by a physical phase plate introduced in
142 the microscope column allows for the maximum contrast in low frequencies, thus
143 producing a better contrast between particles and their background. The main
144 problem of this method is that the image acquisition is in-focus and it is not
145 possible to estimate the CTF, so it is not possible to correct physical aberrations.
146 Danev et al. [55] proposed using the VPP with a bit of defocus. The advantage
147 of this proposal is that the defocus can now be readily be identified through the
148 oscillations of the Thon rings, and its drawback is that the small defocus causes
149 some high frequencies to be damped. The CTF correction for Volta Phase Plate
150 data is available in the three software implementations mentioned earlier.

151 *2.2.2. Particle Picking*

152 Because of the strong background noise, low contrast images, and sample
153 heterogeneity, typically a large number of single-particle images is required for
154 reliable 3D reconstruction. Methods for particle picking from micrographs can
155 be divided into two main categories. The first one is a manual picking process,
156 which is usually a laborious and time-consuming task. It requires a large amount
157 of human effort to obtain a sufficient number of particles that also must be of
158 high quality for high-resolution 3D reconstruction. Moreover, manual picking is
159 considered subjective and can introduce bias and inconsistency.

160 Therefore, currently more popular is the second category consisting of semi-
161 automated and automated methods. This category includes generative ap-
162 proaches, which measure the similarity to a certain reference image. A typical

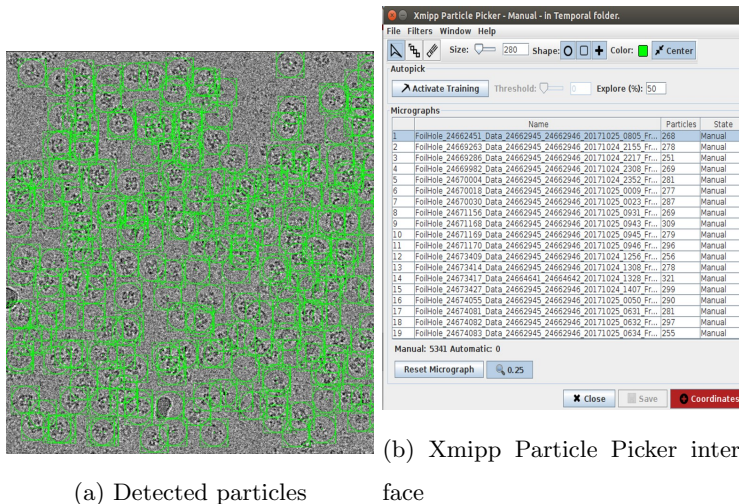


Figure 2: Use of the Xmipp Particle Picker with user input to select single particles. (a) Particles are detected and highlighted in the recorded micrograph. (b) Xmipp Particle Picker interface with a list of all micrographs showing the number of particles found in each micrograph.

163 representative of generative methods is a template-matching technique, which
 164 is employed in RELION [56, 57] or in highly parallel GPU-accelerated gEM-
 165 picker [58]. The input here consists of a micrograph and images containing
 166 2D templates to match. The idea behind template-matching is that the cross-
 167 correlation between a template image and a micrograph is larger in the presence
 168 of the template. Template images could be chosen as a disk with a radius corre-
 169 sponding to the particle size with its edges softened by application of a Gaussian
 170 kernel [59]. Another alternative is *Gautomatch* developed by Kai Zhang [60],
 171 which is a GPU accelerated program for flexible and fully automatic particle
 172 picking from cryo-EM micrographs with or without templates. The automatic
 173 particle picker can learn also from the user the particles of interest by way of
 174 the method given in [61]. This method is available in Xmipp 3.0 software [37],
 175 and an example of use is shown in Figure 2.

176 Since automatic and semi-automatic particle pickers are selecting a non-
 177 negligible number of incorrect particles, particle quality assessment and a sort-

178 ing method based on multivariate statistical analysis of a particle set could be
179 used to separate most erroneously picked particles from correct ones [62]. The
180 problem of discriminating between particles on carbon and particles in ice is
181 solved by detecting carbon supports using *EMHP* package [63].

182 In recent years, deep learning methods start to be employed for particle
183 picking in regular micrographs (not tilted pairs.) *DeepPicker* [64] consists of
184 two modules, where in model training, labeled positive and negative samples are
185 used to train a convolutional neural network (CNN) model, while in the particle
186 picking module, the trained CNN classifier is then used to select particle images
187 from input micrographs. Another recent model also derived from a deep CNN
188 is *DeepEM* [65].

189 In cases when an initial model is not available, a low-to-medium resolution
190 model can be obtained from negatively stained samples by the Random Conical
191 Tilt (RCT) [66] or Orthogonal Tilt Reconstruction (OTR) [67] procedures. The
192 basis for these two methods is in collecting two images of the same sample
193 at different tilt angles, identifying and boxing particles in both images. An
194 accurate solution to finding both the particle correspondence and the tilt-axis
195 estimation was proposed in [68] along with *MaverickTilt* software determining
196 tilt pairs from independent particle coordinates from images [69]. Vilas *et al.*
197 introduced a method of automatically finding correspondences of particles in
198 the untilted and tilted micrographs [70]. The method is available in Scipion
199 [41].

200 2.2.3. Denoising and Image Restoration

201 During the acquisition process, images are usually degraded by blur and
202 noise. Most imaging devices, like CMOS and CCD cameras, are photon counting
203 devices where the resulting noise is non-additive and signal-dependent and it can
204 be modelled by a mixed Poisson-Gaussian (PG) distribution, often encountered
205 also in astronomy [71, 72], biology [73] and medicine [74]. Image restoration
206 methods (CTF correction and denoising) are based on estimating original images
207 from these blurred and noisy observations. In one first step, restoration methods

208 can be separated in two big groups non-blind and blind, depending on whether
209 the Point Spread Function (PSF) is known or not.

210 In addition, the non-blind image restoration techniques can also be broadly
211 categorized into two kinds of approaches [75]. The first is an approach known
212 as *phase flipping*, which involves flipping the sign of the Fourier coefficients at
213 frequencies for whose CTF amplitude is negative, ignoring the effect of the CTF
214 on the Fourier amplitudes. Phase flipping is easy to implement but preserves
215 the noise statistics. The second commonly used approach is Wiener filtering
216 (WF), which takes into account both the phases and amplitudes of the Fourier
217 coefficients. However, to calculate the Wiener filter a prior estimation of the
218 spectral signal to noise ratio (SSNR) of the signal is required, which by itself is
219 a challenging problem.

220 T. Bhamre et al. [76] presented a new approach for non-blind image restora-
221 tion of cryo-EM images based on a modified Wiener filtering. They name it the
222 covariance Wiener filter (CWF) because the main algorithmic step is the esti-
223 mation of the covariance. CWF performs phase and amplitude CTF correction,
224 as well as denoising, thus improving the SNR of the resulting images. In par-
225 ticular, CWF applies Wiener filtering in the data-dependent basis of principal
226 components (*eigenimages*), while traditional Wiener filtering is applied in the
227 data-independent Fourier basis.

228 The first step of CWF is estimation of the covariance matrix of the under-
229 lying clean images, whereas the second step is solving a deconvolution problem
230 to recover the underlying clean images using the estimated covariance.

231 In this statistical model, the Fourier transformed clean images are assumed
232 to be independent, identically distributed (i.i.d.) samples. Since the clean im-
233 ages are two-dimensional projections of a certain three-dimensional molecule in
234 different orientations, the covariance matrix represents the overall image vari-
235 ability due to the three-dimensional structure, the distribution of orientations,
236 and the varying contrast due to changes in ice thickness and structural variabil-
237 ity, which are all of course unknown at this stage. While these model assump-
238 tions do not necessarily hold in reality [77, 78], they simplify the analysis and

239 lead to excellent denoising.

240 The method is thought to deal with images that have an additive white noise,
241 which has equal intensity at different frequencies. However, for a more realistic
242 colored noise process, with different power spectra, the images are processed
243 in order to *whiten* the noise. The noise power spectrum is estimated using
244 the pixels in the corners of the experimental images. One can define a new
245 *effective* CTF including the whiten filter to estimate the new covariance matrix.
246 However, this case is ill-conditioned, and it takes a large number of iterations
247 for the conjugate gradient to converge to the desired solution. Instead, a well
248 conditioned linear system is sought similar to one in the case of white noise.

249 The second step of the CWF is to use the estimated covariance to solve
250 the associated deconvolution problem using Wiener filtering. The result is a
251 denoised and CTF-corrected image for each experimental image.

252 On the other hand, in many situations it is difficult to accurately estimate
253 the PSF (or the CTF) and blind methods may be preferable. B. Bajic et al. [79]
254 presented a novel restoration method for images degraded with PG noise which
255 jointly estimates the original image and the PSF from the observed data. Al-
256 though the method was not designed to process cryo-EM images, they illustrate
257 its applicability in this field.

258 To simultaneously recover the original image and the PSF, the method mini-
259 mizes an objective function. That function firstly contains a term which depends
260 on the targets (clean image and PSF), driving the solution towards the observed
261 data. Secondly, a regularization term which only depends on the clean image
262 provides a noise suppression, whereas a parameter controls the trade-off of the
263 two terms. The role of the regularization term is to provide numerical stability
264 and it may be designed based on the desired characteristics of the unknown
265 image, such as wavelet-based sparsity, smoothness, small total variation, etc.

266 During the clean image estimation, minimization of the objective function
267 is seen as a constrained optimization problem that can be optimized by means
268 of an iterative gradient-based method.

269 *2.2.4. 2D Alignment, Clustering, and Classification*

270 One of the main drawbacks of the cryo-EM single particle analysis is to deal
271 with images with very poor SNR. However, a large number of experimental
272 images is usually acquired. Therefore, averaging all similar and aligned images
273 can substantially enhance the SNR. The averaged images are normally referred
274 to as 2D averages, and they can be used to produce a reliable 3D starting model
275 [80, 81, 82]. The most used methods to simultaneously 2D align and cluster
276 (SAC) are based on the multi-reference alignment (MRA) following a k-means
277 strategy. This strategy involves some randomized initial cluster centers followed
278 with an iterative local-search-based cluster assignment and in-plane rotation
279 [83]. It is possible to employ a previous step of principal component analysis
280 (PCA), so that the clustering is actually performed using a low dimensional
281 representation of the particles, accelerating the process.

282 The results from MRA using k-means strongly depends on the cluster ini-
283 tialization and the number of classes [84], compromising the reproducibility and
284 robustness of the method. C. Reboul et al. [85] presented a stochastic hill climb-
285 ing (SHC) method based on random walks, where the correlation maximizing
286 step of k-means is replaced with the relaxed requirement of identifying *the first*
287 *in-plane rotation and cluster assignment that improves the previous correlation,*
288 *given random sequences of in-plane rotation and cluster assignments.* Thus, the
289 references are randomly ordered and the rotation scan is also performed ran-
290 domly. As soon as a configuration is improving the previous best correlation,
291 the random walk ends and the next particle is processed. Since the cluster cen-
292 ters are not updated until all particles are done, the random walk is performed
293 on all particles independently. The result is faster and less-dependent on the
294 initialization in comparison to previous approaches.

295 Besides improving the SNR, 2D classification can be useful to remove con-
296 taminants. Usually the input dataset is too heterogeneous. The degree of
297 heterogeneity in a cluster can be analyzed using a great variety of procedures,
298 e.g. via PCA of each cluster, obviously after removing the variability caused

299 by image misalignment. Outliers can be identified through their Mahalanobis
300 distance to the centroid [86, 87] of the PCA subspace composed by the first
301 few components. The Mahalanobis distance measures how many standard de-
302 viations away a point is from the mean of a distribution. Images close to the
303 cluster centroid as measured by the Mahalanobis distance form the class core
304 [86].

305 If our 2D clustering is hierarchical [88], the class core can be further refined
306 by considering the subset of images that are basically classified together in
307 the whole hierarchical process. Usually, outliers swap between several classes
308 whereas the true projections tend to remain together in a stable behavior. This
309 refined subset is called stable core. To be more flexible, the implementation can
310 relax this condition. In this way, the stable core is a subset of these particles
311 which have been together for all classification levels (with a certain number of
312 tolerance).

313 The previous methods are devoted to discrete classification; however, this
314 kind of approaches could not be well suited with macromolecules exhibit contin-
315 uous molecular motions. In this situation, several low-resolution maps showing
316 different states of the molecule can guide the alignment and 2D classification of
317 cryo-EM images, e.g. [89].

318 *2.3. 3D Analysis*

319 The 3D reconstruction process can be seen as an optimization problem in
320 which we need to move through a solution landscape where every point repre-
321 sents a 3D model. Each model has an associated energy that depends on the
322 error between that model and the 2D experimental images collected. The aim of
323 this process is to reach the optimal 3D model considering the information car-
324 ried by the 2D cryo-EM images. This task is a main challenge in the field and
325 significant effort has been applied by several researchers to develop algorithms
326 to solve the problem.

327 The whole 3D reconstruction process is commonly managed starting with
328 an initial model estimation, which can be seen as an estimation of the start-

329 ing point in the solution landscape, followed by a refinement to move along
330 the whole landscape, improving the reconstructed model in every step. The
331 refinement algorithms easily get stuck in local minima of the solution landscape
332 [90]. Therefore, a good design of the initial volume estimation and refinement
333 algorithms is key in the accuracy of the final 3D model generated.

334 *2.3.1. Initial model*

335 The goal of the initial model procedure is to create a low-resolution molecu-
336 lar density of the underlying structure, that can be further refined into a high-
337 resolution map. This process is especially important for molecules whose struc-
338 ture is unknown, as using an incorrect initial model can lead to bias in the final
339 map, or slow convergence of the refinement algorithm.

340 In the recent years a plethora of initial model algorithms have appeared and,
341 if 5 years ago the initial volume was an important problem, currently, there are a
342 sufficiently high number of methods such that at least one of them will produce
343 a suitable initial volume.

344 A family of these new algorithms are based on the Central Slice Theorem
345 [91] that states that the Fourier transform of a 2D image belonging to a certain
346 projection direction, corresponds to a slice of the 3D Fourier transform of the
347 volume in the perpendicular direction. So, every pair of the 2D images coming
348 from different projection directions will intersect at a line in the Fourier space,
349 named the common line. The methods [80, 92, 93, 94, 95] are based on this the-
350 orem. [92] described an algorithm based on synchronization to determine the
351 direction of all the 2D images at once. Combining the common lines outcomes
352 for pairs of images, a global assignment of orientations that maximizes the num-
353 ber of satisfied pairwise relations can be derived. The idea of synchronization
354 was further studied in [94] where a graph-partitioning algorithm is suggested
355 to consistently assign orientations, giving a confidence value to each one. One
356 typical problem with these methods is that they are prone to detect false com-
357 mon lines. In [93] a method dealing with this problem is proposed, in which the
358 orientations were estimated by minimization of the sum of unsquared residuals,

359 adding a spectral norm term to avoid the artificial clustering that appears with
360 overlapping slices in the Fourier space. The algorithm proposed in [95] presented
361 a way to model the errors in the estimated common lines giving them a proba-
362 bility value. However, the main drawback of the common lines approaches has
363 not been overcome yet, as they still tend to easily fail when the detection rate
364 of common lines is too low due to the low SNR in typical cryo-EM 2D images.
365 [96]

366 Another usual approach to the initial model problem is to follow a statisti-
367 cal framework, e.g., [97, 82, 98, 99], in which the alignment parameters can be
368 found optimizing some related quantity. [97] presented a probabilistic initial 3D
369 volume generation (PRIME) where each image is assigned to a range of orien-
370 tations with the highest correlations. Then, the 3D initial model is generated
371 giving a weight to every image in every specific orientation proportional to the
372 obtained correlation. The method in [82] is based on dimensional reduction of
373 class average 2D images with the aim of obtaining representative sets of class
374 images with the main structural information. Then, with the 2D representative
375 image sets several initial models are generated. The best initial model can be
376 determined using random sample consensus (RANSAC).

377 [98] was based on Bayesian inference. A pseudo-atomic model is used to
378 represent the 3D structure, whilst the estimation of the unknown 3D structure
379 and image orientations is carried out with a maximum *a posteriori* optimization.
380 However, it must be taken into account that a low number of pseudo-atoms in
381 the pseudo-atomic model could generate inaccurate structural representations.
382 The algorithm presented in [99] followed a maximum likelihood approach where
383 the projection parameters are treated as hidden random variables and the goal is
384 to find the volume that maximizes the likelihood of observing the experimental
385 images (although normally this algorithm is applied to 2D class averages). The
386 method ends up in a weighted least squares problem, in which the weights are
387 given by both the experimental image and the projection direction. Actually,
388 this method introduced an important idea in the field: not only experimental
389 images can vote during the construction of a model by assigning a weight to

390 each projection direction, but projection directions can also vote and help in
391 the decision of the weights of the experimental images.

392 The main drawbacks of statistical approaches are the following: the compu-
393 tational complexity is usually high due to the iterative framework, and, as they
394 need some first estimation to iterate until getting the definitive initial model,
395 tend to easily finish in local minima. This is the problem with a solution land-
396 scape containing plenty of local minima - algorithms may get trapped in these
397 less optimal solutions.

398 In 2018, a new approach to *ab initio* modeling was presented that does not
399 require estimation of the viewing directions of projections. Assuming that the
400 projection orientations are uniformly distributed across the sphere, Levin *et al.*
401 [100] show that a low-resolution estimate is achievable by using just two denoised
402 projections. The authors use Kam’s autocorrelation method and solve for the
403 missing orthogonal matrices by using projection matching. There are a few
404 limitations to this method, one being the assumption that viewing directions are
405 distributed uniformly, as some molecules have preferred orientations. However,
406 the methods shown in this paper may lead model initialization research in a
407 fresh, promising direction.

408 Finally, [101] a particle swarm optimization method is introduced that col-
409 lects different initial volume proposals from other algorithms and considers them
410 to be individuals of a population of initial volumes. Particle swarm optimiza-
411 tion refers to allowing candidate solutions, called ”particles”, to traverse, or
412 ”swarm”, the search space of solutions and approach the optimal solutions. This
413 population is evolved using an algorithm combining stochastic gradient descent
414 and particle swarm optimization. Ordinarily, the whole population converges
415 to a single structure, which is usually a correct initial volume.

416 In many cases, is not possible to build an initial model following the common
417 cryo-EM pipeline. In this situation, it is possible to use negatively stained sam-
418 ples and the Random Conical Tilt (RCT) [66] or Orthogonal Tilt Reconstruction
419 (OTR) [67] procedures, obtaining a low-to-medium resolution model.

420 Although there is a wide range of possibilities to tackle the initial volume

421 estimation, this is still an open problem, but to a much lesser extent than it was
422 five years ago. More robust algorithms are still in need, since there are situations
423 in which the existing algorithms are not able to produce a satisfactory result.

424 2.3.2. Refinement and Reconstruction

425 One key step in the cryo-EM image processing pipeline is the 3D reconstruction
426 of a model compatible with the available 2D images coming from projections
427 of the molecule under study, achieving a resolution sufficiently to interpret de-
428 tails in the macromolecular structures. This is the problem that refinement and
429 reconstruction methods try to solve.

430 Despite the fact that 2D projection images are contaminated by a huge
431 amount of noise, thanks to the large number of available images in SPA, the
432 averaging of many images coming from the same direction is able to greatly
433 reduce the noise level, making the reconstruction process mainly limited by
434 incomplete coverage of the viewing directions, limiting effects of the CTF, and
435 execution time. We can find plenty of reconstruction methods, mainly organized
436 in two families: direct Fourier inversion and iterative algorithms.

437 Direct Fourier inversion methods are based on the Central Slice Theorem
438 [91]. They are well suited to handle a large number of projections, which is
439 common in SPA, with a reasonable computational burden and high accuracy
440 when the angular coverage of the set of projections fully fills the 3D Fourier
441 space. However, when we do not have a good angular coverage the outcomes
442 generated by these methods cannot be optimal solutions. Abrishami *et al.* [102]
443 dealt with the angular coverage problem by introducing a gridding-based direct
444 Fourier method that used a weighting technique to compute a uniform sampled
445 Fourier transform. This proposal followed the general idea of [34] and added a
446 weighting scheme in which every projection direction with weights is estimated
447 in an iterative way - evaluating a function similar to a kernel interpolator.

448 Another research line has sought to incorporate *a priori* information in the
449 3D reconstruction process. Some iterative procedures have exploited sparse
450 representation of the reconstructed volume. For instance, Moriya *et al.* [103]

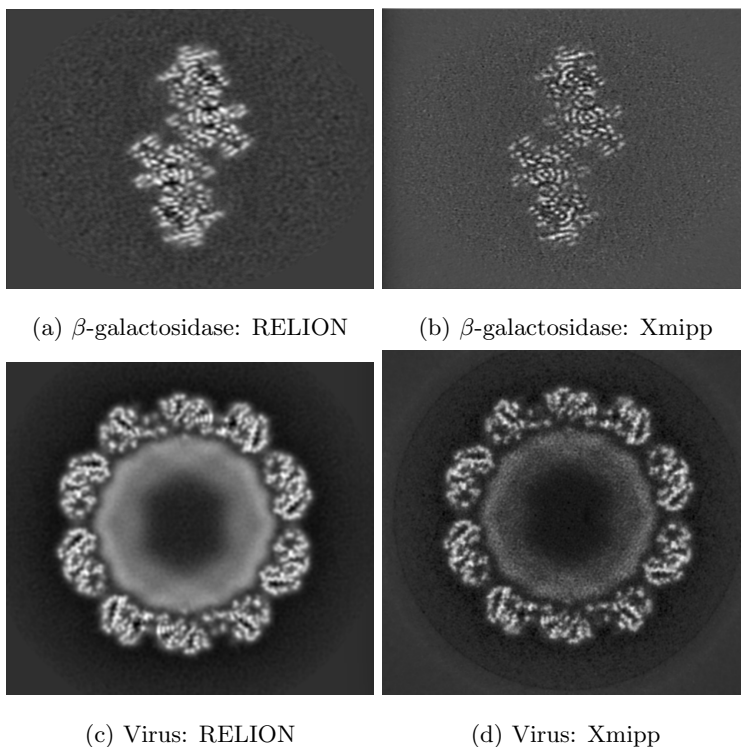


Figure 3: Examples of two reconstructed structures using RELION autorefine (*left*) and Xmipp highres (*right*). Despite the input data were the same, both algorithms cast different degree of detail keeping the same structure. The representative slices from 3D reconstruction of β -galactosidase (EMDB entry 10013) (*top*) and Brome Mosaic Virus (EMDB entry 10010) (*bottom*)

451 assumed a Median Root Prior which favored locally monotonic reconstructions.
 452 Xu *et al.* [104] used an improved L^2 gradient flow method (L2GF) in which
 453 an energy functional consisting of a fidelity term and a regularization term was
 454 employed. For a review of iterative algorithms, the interested reader is referred
 455 to [105]. The use of different reconstruction algorithm depends on the user,
 456 because they might cast slightly but non-negligible results, an example showing
 457 two reconstruction methods is shown in Figure 3.

458 The main drawback of existing refinement and reconstruction methods is
 459 the difficulty of managing the projection images. There are a limited number

460 of projection images available, which impedes the ability to correctly pose the
461 inverse problem. Another drawback is the high computational cost, even when
462 using highly optimized implementations on graphic processing units (GPUs).

463 More general statistical methods are gaining popularity recently. [106] pro-
464 posed a novel speedup of the expectation-maximization algorithm. The idea be-
465 hind the approach was to represent the 2D experimental images and the model
466 projections in two low-dimensional subspaces. The matching between experi-
467 mental and projections images was performed in the subspace bases. Because
468 the number of basis elements is much smaller than the number of images and
469 projections, substantial speedup was achieved. The main difference between
470 this algorithm and that proposed in [34] is that the latter is implemented in the
471 Fourier domain whilst the subspace in [106] can be applied in Fourier or spatial
472 domains. In [107] the stochastic gradient descent (SGD) and Bayesian marginal-
473 ization algorithms were used to recover multiple 3D states of the molecule. The
474 algorithm started with an arbitrary computer-generated random initialization
475 that was incrementally refined with random selection of 2D images. The main
476 problem of this algorithm, since it essentially relied on an arbitrary initial map,
477 was the sensitivity to be biased towards the initial map, although the SGD is
478 supposed to help in this regard.

479 *2.3.3. Molecule Heterogeneity*

480 Macromolecules can undergo conformational changes due to their functional
481 needs and the interaction with other molecules and the environment. For this
482 reason, in the 2D cryo-EM images it is possible to visualize different molecule
483 conformations, which poses a great challenge in the development of processing
484 algorithms to analyze the molecular structures. Heterogeneity is currently an
485 active field of research in cryo-EM as to get the highest resolution in the 3D
486 model reconstruction is essential to discover the presence of different conforma-
487 tions. In this review, we divide the approaches into four main families: physical,
488 statistical, covariance analysis, and projection subtraction methods.

489 In the physical approaches we can find a family of algorithms based on

490 anisotropic network model (ANM), which is a direct application of the normal
491 mode analysis, and molecular dynamics (MD) to predict the collective motions
492 of structures and to describe full atomic molecular motions, respectively. [108]
493 combined both with Monte Carlo/Metropolis scheme to randomly select the
494 modes to deform the structure with the aim of generating trajectories between
495 two conformational states. In [109] ANM and MD were also used to couple
496 local and global motions efficiently. The method performed a large number of
497 MD simulations, each of them corresponding to the excitation of a randomly
498 determined linear combination of selected normal modes. Similarly, in [110]
499 combinations of ANMs were used to calculate the conformational space for a
500 molecule, and a clustering procedure was applied to construct representative
501 substates.

502 Among the statistical approaches is a method for sorting structural states
503 found in [111]. It was based on bootstrapping of 3D sub-ensembles and 3D mul-
504 tivariate statistical analysis followed by 3D classification. In [112] a method to
505 analyze distances among elastically aligned pairs of EM models was presented.
506 Each experimental 3D model was transformed by elastic deformation and com-
507 pared with other models in terms of structural and conformational differences.
508 Punjani *et al.* [107], that was described in the previous section, was also de-
509 veloped to refine multiple high-resolution 3D models directly from single parti-
510 cle images using SGD and Bayesian marginalization algorithms. [113] studied
511 the conformational variability combining an iterative 3D classification approach
512 with 3D principal component analysis (PCA). 3D classification gave hundreds
513 of 3D structures, which were ordered according to their conformational similar-
514 ities by applying PCA. Thus, this method is able to identify motion patterns
515 of flexible components in a conformational landscape. An example is shown in
516 Figure 4.

517 A different approach to discover heterogeneity in cryo-EM data consists of
518 estimating the covariance of the reconstructed model. [114] proposed a new
519 estimator in the Fourier space that converges to the population covariance ma-
520 trix as the number of images grows, but this method involves the inversion of a

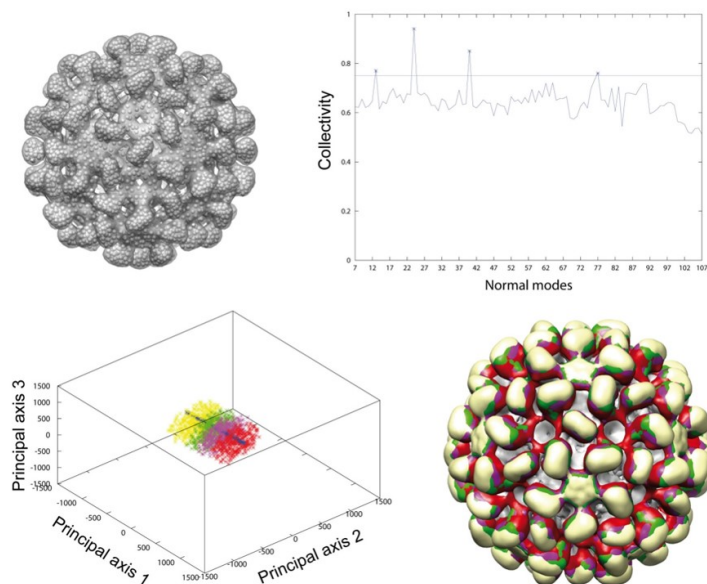


Figure 4: *Top, left:* 3D Electron density map of the Tomato Bushy Stunt Virus and its pseudoatomic representation. *Top, right:* collectivity of the normal modes of the pseudoatomic representation. *Bottom, left:* projection of the deformation parameters estimated for experimental images onto a 3D Principal Component (PCA) Space. Clustering of these projections into 4 classes. *Bottom, right:* The corresponding reconstructions of the 4 identified classes in the PCA space are shown; their isosurface representation is superposed using the same colors than the identified classes, exhibiting a conformational change.

521 high-dimensional linear operator. In [115], instead of inverting the original lin-
522 ear operator, it was proposed to use the conjugate gradient, achieving a lower
523 computational complexity and the possibility of including the CTF correction.
524 [116] estimated the whole covariance matrix, instead of only its main eigenvec-
525 tors. Hence, this approach avoided the resampling problem and enabled the
526 analysis of covariance in localized regions.

527 The work described in [117] used fluctuation-dissipation theory for estimat-
528 ing a spring-and-mass mechanical model. Thus, this approach was able to trans-
529 form the covariance matrix into a generative mechanical model of the complex.

530 The last family of methods to deal with structural heterogeneity is based
531 on focusing the refinement process on the region where the motion is mostly
532 taking place, masking out the fixed parts of the images. This procedure is usu-
533 ally named projection subtraction and it is able to take into account during
534 3D refinement only those parts of the images where the structural variability
535 can be found. [118] proposed to subtract projections of the fixed part of the
536 molecule from every experimental image. This way, the modified experimental
537 image only contains the moving part of the molecule. This procedure required
538 knowledge of the relative orientation of each particle, which was obtained from
539 a consensus refinement of the entire data set against a single, unmasked refer-
540 ence. A similar idea was published in [119], where a first 3D estimated model
541 was separated into different modules according to prior knowledge. For every
542 module, the orientation parameters were calculated by maximizing the cross-
543 correlation coefficient. However, this method assumed that the resolution of the
544 initial 3D model was high enough to discriminate different modules. One of the
545 main drawbacks of the projection subtraction approaches is that the moving
546 element needs to be rigidly moving and of enough size so that the subtracted
547 projections can be correctly aligned.

548 Despite all the research in heterogeneity, the main difficulties remain. First,
549 the 3D models need to be reconstructed from 2D images, making it difficult to
550 connect the models reconstructed from thousands of 2D experimental images
551 with the actual conformational state associated to a projection. Moreover, the

552 noise problem must be highlighted, as 2D experimental images have a SNR
553 well below 1 (which means that there is much more noise power than signal
554 power). This problem poses a limit on the resolution that can be achieved
555 in the 3D models reconstructed with SPA, making some conformational states
556 indistinguishable.

557 *2.3.4. Validation of Results*

558 The reconstruction workflow involves many steps in which the user decisions
559 might determine the quality or even the validity of the electron density map.
560 The low SNR of cryo-EM images complicates the reconstruction process. In
561 particular, it can induce problems in critical steps, especially in the angular
562 assignment of particles. Thus, low quality maps can be obtained or, in the
563 worst case, a wrong map can be elucidated. The map validation can be carried
564 by means of external techniques as X-rays or NMR, or alternatively by using
565 the experimental images that must be in agreement with the volume. A set of
566 methods addressed to validate the map have been proposed.

- 567 1. *Overfitting detection:* Overfitting phenomena occurs particularly at high
568 resolution. A reconstructed volume using noisy particles should stand
569 out in the resolution of the map. By substituting a certain number of
570 experimental particles by noisy particles and reconstructing, a validation
571 can be carried out [120]. The goal will be to analyze the resolution of
572 the reconstructed volume before and after noise substitution. If both
573 resolutions are consistent, then an aligning problem is detected.
- 574 2. *Tilt Pairs Validation:* This was the first validation method [121, 122, 123]
575 and requires a measurement of the sample at two different tilt angles.
576 The geometry constraint introduced by the tilt angle and direction must
577 be conserved when the particle's tilt pairs are aligned with the obtained
578 volume, i.e. the angular relation between the untilted and tilted particle.
579 The results of the angular alignment are simply plotted in a polar plot,
580 in which the radial measure represents tilt angle and the angle shows
581 the tilt direction. When the volume is in agreement with the angular

582 alignment, the plot will exhibit a cluster. The high level of noise might
583 introduce non-negligible alignment errors which are shown as scattered
584 points in the polar plot; to analyze the existence of clusters an statistical
585 approach is required [124].

586 3. *Alignability validation*: These methods aim at measuring the alignability
587 of the set of images used for reconstruction [125, 126]. Leaving out sym-
588 metrical issues, each particle will be a map projection under one direction
589 and it is expected that the most probable orientations for each particle
590 form a cluster in the projection sphere. Additionally, if we make a *de novo*
591 angular assignment, it is expected that the new angular assignment is con-
592 sistent with the angular assignment used for reconstruction. In contrast,
593 pure noise images are expected to behave in the opposite way: the most
594 probable directions are not clustered, and the *de novo* angular assignment
595 does not coincide with the assigned angles.

596 4. *Atomic model Validation*: Many structures elucidated by cryo-EM were
597 previously obtained by other techniques such as X-ray crystallography or
598 NMR. In these cases, the atomic model is known. Then, the electron den-
599 sity map must follow the atomic model at least at medium-low resolution.

600 2.4. Resolution

601 Once the macromolecular structure has been obtained and validated, it is
602 necessary to report a quality measurement of its electron density map. The
603 resolution tries to answer this regard. There is no consensus about a universal
604 definition of resolution, the most widespread being the size of the smallest reli-
605 able detail in the map. However, from an optical point of view, resolution has a
606 clear definition as the capability of an imaging system of distinguishing two sep-
607 arated points in an acquired image. The Rayleigh criterion can be considered as
608 the standard in optics [127]. It should be highlighted that this definition implies
609 that resolution is a property of the imaging system instead of a property of the
610 acquired image (map in cryo-EM). Nevertheless, when the imaging system is
611 omitted and only the image is analyzed, other criteria are used, e.g., Johnson

612 criteria [128].

613 In cryo-EM, the resolution has been traditionally analyzed in a global sense,
614 that is, reporting a single parameter called global resolution that summaries the
615 quality of the map. For a comprehensive review of these resolution measures,
616 the reader is referred to [129]. The most used global resolution method is the
617 Fourier Shell Correlation (FSC) where the correlation of two band-pass filtered
618 independent reconstructions is measured. The resolution is defined as the central
619 frequency of the band-pass filter at which the correlation drops below a given
620 threshold. The problem with this measure is that it is a self-consistency measure
621 of the reconstruction process, rather than a quality measure of the reconstructed
622 volume, e.g. it rewards systematic errors during the reconstruction process. To
623 do that, the *Gold Standard* procedure is carried out. It consist in splliting the
624 set of particles in two sets, and then performing two independent reconstructions
625 [130, 131]. This is a self-consistency measurement because both reconstructions
626 should cast similar maps. If one of the reconstructions exhibits overfitting,
627 it will not correlate with the other. Despite the gold standard, there is still
628 some overfitting. In this regard, the phase-randomization method can be used
629 to calculate the true FSC-resolution by noise substitution of particle phases
630 beyond a certain frequency [132]. Cryo-EM images present low SNR and even
631 particles of noise can be aligned i.e. features of noise correlate with the reference
632 [133, 134, 120], in particular at high frequencies. When many particles of noise
633 are aligned, those poor features are reinforced and a model bias is introduced.
634 This problem is called the *phantom in the noise* or *Einstein from noise*.

635 However, as the pioneers of the local resolution showed, one number does not
636 fit all [135]. It has been shown that resolution is actually a tensor (it depends
637 on the location within the volume and the direction) [129], and the global reso-
638 lution summarizes this rich information into a single number. The local quality
639 differences have their origin in the reconstruction process. The SPA workflow
640 considers that all particles (projections of the macromolecular complex) are
641 identical and uniformly distributed on the projection sphere. Unfortunately,
642 reality differs from this assumption because of heterogeneity and angular orien-

643 tation. The heterogeneity has been identified as one of the main problems in
644 cryo-EM [136], and contradicts the SPA hypothesis that all particles are iden-
645 tical copies of the same complex. Thus, we distinguish heterogeneity due to 1)
646 the macromolecular complexes not being rigid and presenting a certain degree of
647 flexibility, i.e. conformational heterogeneity; 2) despite the purification efforts
648 some proteins present slight, but not negligible, structural heterogeneity. Radi-
649 ation damage can also be responsible for this kind of heterogeneity. In any case
650 the heterogeneous region of the macromolecule will be blurred. The angular
651 assignment of particles is the second main source that induces local variations
652 in the electron density map. If the sample presents preferred directions or even
653 lack of information in others, the distribution of angular assignments will be
654 non-uniform, and will cast better solved directions than others [137]. To over-
655 come this problem of angular coverage, [138] showed that by tilting the sample
656 the overall resolution can be increased and the quality map improves.

657 *Blocres* was the first method for estimating local resolution maps in cryo-
658 EM [135]. It extends the FSC measurement in a local sense. Thus, by means of
659 two half maps and a moving window centered in the interest voxel a local FSC
660 can be calculated. The critical point is to set the window size. Logically, this
661 is a self-consistency measurement, as the FSC itself, and it preserves all FSC
662 properties. Interestingly, *Blocres* introduced the possibility of computing the
663 locally filtered map at the local resolution values.

664 Nowadays, the most spread method in local resolution measurements is
665 *ResMap* [139]. Its rationale is the local detection of a sinusoidal signal above
666 the noise level in a statistical sense. This task is carried out by means of a
667 steerable function basis that allows for modeling of sinusoidal signals by means
668 of linear combinations. Moreover, this method overcomes the drawback of using
669 two half maps by computing local resolution maps using just a single volume
670 or two half maps. In addition, it considers the spatial correlation in terms of
671 resolution between closest voxels and computes a False Discovery Rate i.e. in
672 an hypothesis the expected value of the number of resolutions wrong assigned
673 over the total number of resolution assigned.

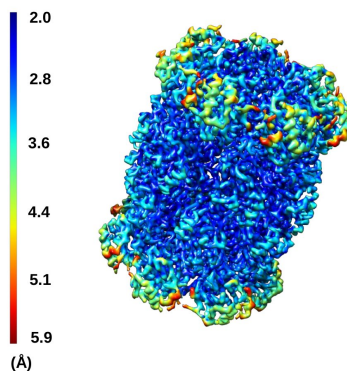


Figure 5: Local resolution map of the *Thermoplasma acidophilum* 20S proteasome using the MonoRes method [140].

674 Recently, a new method called *MonoRes* for estimating local resolution has
 675 been published [140]. The idea of this method is to measure the local energy of
 676 the macromolecule and the energy distribution of the noise. The discrimination
 677 between noise and particle is provided by a mask. Thus, a frequency sweep
 678 is carried out performing hypothesis tests to determine if the energy of each
 679 voxel in the filtered map is significantly higher than the energy of noise at
 680 that frequency. This new method has the advantage of being fully automatic
 681 without user intervention, computationally faster than other approaches, and
 682 invariant under b-factor correction, and any other isotropic frequency correction.
 683 In addition, it also provides a local filtered map at the local resolution values,
 684 shown in Figure 5.

685 2.4.1. Fitting an Atomic Model

686 Thus far, we have discussed methods for building and refining a 3D recon-
 687 struction of the molecule being imaged. This reconstruction is in reality just
 688 a density map. The ultimate interest in the research community is focused on
 689 an atomic level structural model of the macromolecule. Initially, a fitting can
 690 be performed for secondary structure elements (SSEs) such as α -helices and β -
 691 sheets. Initial methods from the early 2000s focused on one particular SSE for
 692 search, but in more recent years, with SSELearner (2012) and the like, different

693 SSE types can be resolved using just one method [141]. There are different ap-
694 proaches to fitting multiple SSEs. SSELearner uses a local structure tensor to
695 characterize shape at density voxels. A support vector machine is trained with
696 discriminatory tensors and known SSEs. This learning approach uses previously
697 solved structures to solve similar unsolved molecular structures. [142]

698 When fitting to 3D density maps, both rigid fitting and flexible fitting mech-
699 anisms can be used. Rigid fitting is often used as a precursor to flexible fitting,
700 which then makes allowances for conformational changes. These changes oc-
701 cur especially during interaction of the protein with other proteins. Another
702 precursor to flexible fitting can be coarse graining. Coarse graining combines
703 multiple atoms based on neighborhood arrangement into psuedoatoms that can
704 be arranged into a low resolution model. This can save computational energy
705 when modeling large molecules. [143] The coarse grained model can then be
706 refined, like rigid fitting, with flexible fitting - flexible fitting requires search
707 of the solution space of possible conformations. Many methods use simulated
708 annealing to find the best fit [144].

709 Best fit can be determined using a variety of metrics, the oldest being cross-
710 correlation between the estimated structure and the density reconstruction.
711 Different metrics have been proposed over the years, including surface area
712 agreement with the density model, stereochemistry metrics considering atomic
713 bonding and van der Waals forces, and others. Recent work has shown that a
714 combined metric of local mutual information and amount of overlap with the
715 density reconstruction performs better than cross-correlation alone [145]. It
716 seems that along with validation methods for 3D reconstructions, evaluation of
717 atomic models is a promising direction for cryo-EM research.

718 Atomic model refinement is also a popular topic of current research which
719 goes hand in hand with model evaluation. Current work improves fitting of
720 amino acid sidechains by using multiple local optimization results instead of
721 one global optimization result [146]. For model refinement, researchers have
722 also analyzed physical properties that should be taken into consideration, such
723 as partial charges on atoms [147].

724 Building an accurate atomic model is possible even without a reliable 3D den-
725 sity map. As noted in previous discussions, we know that molecules have certain
726 preferred orientations within a grid. If the set of orientations only includes a
727 few possible rotations, then 3D reconstruction through traditional methods is
728 intractable. Traditionally in these situations, 2D class averages are compared
729 to candidate models, which are represented by a graph of SSE components and
730 amino acid side-chains [148]. Comparisons are performed based on similar met-
731 rics as when fitting to density maps. More recently, in 2015, electron atomic
732 scattering factors (EASF) have been used to generate 3D EM volumes from
733 atomic models. The EASF for each element represents the shape of atoms as
734 seen by electrons in the electron beam, and is related to the elastic scattering
735 of electrons. These EASF functions can be sampled to create an atomic model
736 of a macromolecule, that can then be used with any of a number of popular
737 software tools to generate a density map of the molecule. [78]

738 Another exciting new direction for atomic model fitting is to find the pathway
739 of conformational change. Matsumoto et al. generate various atomic models
740 with different conformations, which are then deconstructed into their hypothet-
741 ical prior 2D projections. The projections are compared to actual projection
742 images, building a distribution of conformations from the best matches. From
743 this distribution, the path of conformational changes that a protein undergoes
744 can be estimated, which is important for understanding functional relationships.
745 [149]

746 **3. Conclusions - Current Image Processing Challenges**

747 Despite the recent successes of cryo-EM, this modality is still a very ac-
748 tive research area, and experimental advances are still in development including
749 sample preparation [7], camera detection efficiency [7, 136, 150], specimen stabi-
750 lization under the beam [150], better electron optics (energy filters, aberration
751 corrections) [151, 152, 153], in-focus phase contrast [7], computational means to
752 validate structures [154, 7, 136], wider access to high-end microscopes [7, 150],

753 and better training [7]. From the data analysis point of view, we would like to
754 complement this list with the following considerations:

- 755 1. Better BIM correction: Specimen movement under the electron beam is a
756 serious issue. The steady progress in this area is clear and positive, with
757 proposals at the level of sample preparation [155, 156], computational
758 frame alignment [157] and dose weighting [43, 158]. However, the best
759 way to combine all these approaches is still unclear, and even some BIM
760 effects, such as out-of-plane rocking along beam direction, are not yet
761 addressed by any method.
- 762 2. Finer aberration corrections: Microscope aberrations that have not been
763 corrected by hardware must be estimated and corrected by software. Many
764 attempts have been made to correct for spherical aberrations [159], mag-
765 nification anisotropy [160], or local defocus changes [161], but their use
766 is not widespread, probably indicating that still a better match into the
767 processing workflow is required. Even such a basic task as focus deter-
768 mination is far from trivial and reliable for high resolution [162]. Ad-
769 ditionally, the weak-phase approximation is violated for large specimens,
770 and at high resolution the Central Slice Theorem does not hold as an
771 image formation model [151, 14, 16]. This implies that beyond a given
772 resolution, reconstruction algorithms are not correctly handling frequency
773 coordinates. Finally, the much anticipated introduction of phase plates
774 as a way to avoid defocusing [163] poses additional challenges, since focus
775 determination in these conditions is especially difficult.
- 776 3. Handling homogeneity/heterogeneity and flexibility: Particle flexibility and
777 heterogeneity is at the same time a blessing and a curse of EM. On one
778 side, flexibility helps to reveal the dynamics of the macromolecule under
779 study. On the other side, only homogeneous sets of particles can be re-
780 constructed to atomic resolution. The compromise between a data set
781 being as large as possible and as homogeneous as possible is still an open
782 problem, particularly due to the low contrast and SNR of the acquired im-

783 ages. Significant advances in this regard have been made in recent years
784 [57, 164]. However, the issue is far from settled, particularly in those cases
785 in which conformational changes correspond to a continuous distribution
786 of states. This issue has been explored in some works [165, 89], but this
787 problem still needs further investigation. A particularly challenging situa-
788 tion occurs when studying a macromolecule of unknown structure. Indeed,
789 most image classification algorithms are designed as local optimizers that
790 start from a reasonably good initial map. If this map is not available, al-
791 gorithms may easily find nonsensical structures. There are specific initial
792 volume algorithms to handle this issue [166]. However, currently, there is
793 no algorithm specifically designed with flexibility/heterogeneity in mind.

794 4. Complement with other information sources: With very few exceptions
795 [167], current reconstruction processes do not consider any source of in-
796 formation other than the projection images produced by the microscope.
797 After a 3D map is obtained, modeling - especially the modeling of large
798 macromolecular complexes - certainly benefits from other sources of in-
799 formation, such as cross-linking and mass spectroscopy [168] or protein-
800 protein interaction data [169]. However, the explicit algorithmic incorpo-
801 ration of *a priori* information about the type of signals (macromolecular
802 maps) being handled is missing in the field.

803 5. Validation: For the good and for the bad, data analysis always produces
804 a model of the macromolecular structure. Unfortunately, due to the high
805 level of noise and the high dimensionality of the optimization process,
806 the chances of getting trapped in a local minimum are not negligible.
807 There are two possible manifestations of a local minimum: 1) the overall
808 shape of the structure is incorrect (despite the fact that its projections
809 are compatible, to a certain degree, with the experimental images); 2)
810 small details of the structure are incorrect (the algorithm has overfitted
811 noise). The first problem can be alleviated if similar maps are obtained
812 when starting from several initial models. However, automatic algorithms
813 capable of detecting this situation are still in need [122, 120, 125, 126].

814 The second case can be alleviated by independently processing two halves
815 of the data [170]. But the field needs better data processing strategies
816 that do not imply using only a half of the dataset at hand.

- 817 6. Standardization: Thanks to the success of cryo-EM as an imaging tech-
818 nique, many engineering groups are getting involved in the global research
819 effort and adding new small pieces of software solving specific problems. In
820 addition, we have the traditional software packages that cover the whole
821 image processing pipeline (Relion [171], Eman [172], Xmipp [173, 37],
822 Spider [38], Imagic [174], Frealign [175], ...) and systems that integrate
823 algorithms from multiple sources (Appion [42] and Scipion [41, 176]). This
824 ecosystem of software lacks a common standard of interchanging informa-
825 tion. Although some attempts have been proposed at the level of metadata
826 [177] and geometry [178], they have not been widely adopted. Addition-
827 ally, the field is lacking a mechanism to report the image processing steps
828 carried out from the acquired movies to the final 3D reconstruction.
- 829 7. Data Management: The number of solved structures is growing year af-
830 ter year. Thus, the structural biology community and in particular EM-
831 community is getting awareness about sharing this information. To achieve
832 that, there are some web services as they are: The EMDatabank (<http://www.emdatabank.org>),
833 Worldwide Protein Data Bank (wwPDB; <http://wwpdb.org>). Other databases
834 such as EMPIAR (<http://www.ebi.ac.uk/pdbe/emdb/empiar/>) pursues
835 raw data availability. For a good review on data management and databases
836 in structural biology see [179].

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